# Tensor Response Regression and Neuroimaging Analysis

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### Outline

- talk outline:
  - overview
  - motivating examples
  - tensor response regression: sparsity and low-rankness
  - tensor response regression: generalized sparsity and envelope approach
- collaborators:
  - William Jagust Lab @ UC Berkeley
  - Will Wei Sun @ U Miami; Xin Zhang @ FSU
- thanks:
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  - NIH 2R01AG034570-06A1 (PI: Jagust)



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  - even my in-laws got interested in what I am doing...



#### imaging modalities:

- anatomical magnetic resonance imaging (MRI), functional magnetic resonance imaging (fMRI), positron emission tomography (PET), electroencephalography (EEG), ...
- a unifying form: multidimensional array, a.k.a. tensor





- neuroimaging problems under investigation:
  - tensor regression
    - tensor predictor regression
    - tensor response regression
  - brain connectivity analysis
    - graphical model estimation (undirected, directed, Gaussian, non-Gaussian, static, dynamic)
    - graph inference
    - graph based regression (association) analysis
  - multimodal neuroimaging analysis
    - integrative classification
    - correlated region identification and inference
  - more topics
    - longitudinal imaging analysis
    - imaging genetics
    - imaging causal inference



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#### pick up another new topic here?

- ► attention deficit hyperactivity disorder (ADHD) study:
  - ▶ one of the most commonly diagnosed child-onset neurodevelopmental disorders, with an estimated childhood prevalence of 5 10% worldwide
  - ▶ 776 subjects: 285 combined ADHD subjects and 491 normal controls
  - anatomical MRI images were acquired and preprocessed
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- autism spectrum disorder (ASD) study:
  - an increasingly prevalent neurodevelopmental disorder; 1 in 68 american children according to CDC in 2015
  - ▶ 795 subjects: 362 ASD subjects and 433 normal controls
  - functional MRI images were acquired and preprocessed into 2 forms
  - ► fractional amplitude of low-frequency fluctuations (fALFF), which characterizes the intensity of spontaneous brain activities, and is in the form of 3D array, 91 × 109 × 91
  - partial correlation between brain regions of interest, which describes the conditional dependency and synchronization of brain systems, is in the form of 2D symmetric matrix, 116 × 116

- scientific question of interest:
  - understand the change of the tensor image or brain connectivity pattern as the predictors such as disease status varies, after adjusting for the demographical and other variables
  - identify brain regions exhibiting different patterns across subject groups
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- statistical formulation: tensor response regression
  - predictors: binary diagnostic status, age, gender, ...
  - response: 3D MRI, 3D fALFF, 2D symmetric connectivity matrix
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  - solution I: generalized sparsity and envelope approach
  - solution II: sparsity and low-rankness



# Generalized sparsity and envelope



# Model

model:

$$oldsymbol{Y} = oldsymbol{B} imes_{(D+1)} oldsymbol{X} + arepsilon$$

- $\mathbf{Y} \in \mathbb{R}^{r_1 \times \cdots \times r_D} = D$ th-order array-valued response; e.g., MRI scan
- $X \in \mathbb{R}^p$  = group indicator, plus additional covariates like age, gender
- $\boldsymbol{B} \in \mathbb{R}^{r_1 \times \cdots \times r_D \times p} = (D+1)$ th-order coefficient tensor that captures the interrelation between Y and X, and is our parameter of interest
- ►  $\times_{(m+1)}$  is the (m+1)-mode product of the tensor **B** and vector **X** ►  $\varepsilon \in \mathbb{R}^{r_1 \times \cdots r_D} = m$ th-order error tensor independent of **X**
- $vec(\varepsilon) \sim Normal(0, \Sigma)$ , where the covariance has a separable Kronecker covariance structure such that

$$\operatorname{cov}\{\operatorname{vec}(\boldsymbol{\varepsilon})\} = \boldsymbol{\Sigma} = \boldsymbol{\Sigma}_D \otimes \cdots \otimes \boldsymbol{\Sigma}_1$$

normality is not essential



▶ assumption: there exist subspaces  $S_d \subseteq \mathbb{R}^{r_d}$ , d = 1, ..., D, st

- ▶  $P_d \in \mathbb{R}^{r_d \times r_d}$  is the projection matrix onto  $S_d$ ,  $Q_d = I_{r_d} P_d$  is the projection onto the complement space  $S_d^{\perp}$
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- sparsity principle in variable selection: a subset of individual predictors are irrelevant to the regression
- generalized sparsity principle: shares the same spirit that only part of information is deemed useful for regressions and the rest irrelevant, but is also more flexible in that it permits linear combination of the variables to be irrelevant

#### **Tensor envelope**

- why helpful?
  - ▶ dimension reduction on **Y**: let  $\Gamma_d \in \mathbb{R}^{r_d \times u_d}$  be a basis for  $S_d$ , and  $\Gamma_{0d} \in \mathbb{R}^{r_d \times (r_d u_d)}$  the complement basis

$$\boldsymbol{Y} \in \mathbb{R}^{r_{\boldsymbol{1}} \times \cdots \times r_{\boldsymbol{D}}} \Rightarrow [\![\boldsymbol{Y}; \boldsymbol{\Gamma}_{1}^{\mathsf{T}}, \dots, \boldsymbol{\Gamma}_{\boldsymbol{D}}^{\mathsf{T}}]\!] \in \mathbb{R}^{u_{\boldsymbol{1}} \times \cdots \times u_{\boldsymbol{D}}}, \quad u_{d} \leq r_{d}$$

number of free parameters:

- difference:  $p\left\{\prod_{d=1}^{D} r_d \prod_{d=1}^{D} u_d\right\}$
- more efficient than OLS
- tensor response envelope:

$$\mathcal{T}_{\Sigma}(\boldsymbol{B}) \equiv \mathcal{E}_{\Sigma_{D}}\left(\boldsymbol{B}_{(D)}
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> number of free parameters: — e.g.,  

$$r_1 = r_2 = r_3 = 64, u_1 = u_2 = u_3 = 10, p = 3$$
  
> before:  $p \prod_{d=1}^{D} r_d + \sum_{d=1}^{D} r_d(r_d + 1)/2$  — 792, 672  
> after:  
 $p \prod_{d=1}^{D} u_d + \sum_{d=1}^{D} \{u_d(r_d - u_d) + u_d(u_d + 1)/2 + (r_d - u_d)(r_d - u_d + 1)/2\}$   
— 9, 240  
> difference:  $p \{\prod_{d=1}^{D} r_d - \prod_{d=1}^{D} u_d\}$  — save 783, 432 parameters

- more efficient than OLS
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# Estimation

- estimation:
  - maximum likelihood estimation: iterative optimization algorithm
  - approximation: one-step optimization algorithm

for  $s = 0, \ldots, u_d - 1$  do set  $G_d^s = 0$  if s = 0 and  $G_d^s = (g_{d1}, \ldots, g_{ds})$  otherwise construct  $G_{0d}^s$  as an orthogonal basis complement to  $G_d^s$  in  $\mathbb{R}^{r_d}$ solve the objective function over  $w \in \mathbb{R}^{r-s}$  subject to  $w^T w = 1$ :

$$\begin{aligned} \mathbf{w}_{d+1} &= \arg\min_{\mathbf{w}} \log \left\{ \mathbf{w}^{\mathsf{T}} \left( (\mathbf{G}_{0d}^{s})^{\mathsf{T}} \mathbf{\Sigma}_{d}^{(0)} \mathbf{G}_{0d}^{s} \right) \mathbf{w} \right\} + \\ &\log \left\{ \mathbf{w}^{\mathsf{T}} \left( (\mathbf{G}_{0d}^{s})^{\mathsf{T}} \mathbf{N}_{d}^{(0)} \mathbf{G}_{0d}^{s} \right)^{-1} \mathbf{w} \right\} \end{aligned}$$

set  $\pmb{g}_{d+1} = \pmb{G}_{0d}^s \pmb{w}_{d+1} \in {\rm I\!R}^{r_{\pmb{d}}}$  and normalize to unit length end for

envelope dimension estimation: a variant of BIC



#### Theory

asymptotics:

assuming  $\operatorname{vec}(\boldsymbol{\varepsilon}_i)$ ,  $i=1,\ldots,n$ , are i.i.d. with finite fourth moments

- consistency:  $\widehat{B}_{\rm ENV}^{it}$  and  $\widehat{B}_{\rm ENV}^{os}$  both converge at rate- $\sqrt{n}$  to the true tensor coefficient  $B_{\rm TRUE}$
- ► asymptotic normality:  $\sqrt{n} \text{vec}(\widehat{B}_{\text{ENV}}^{it} B_{\text{TRUE}}) \rightarrow N(0, U_{\text{ENV}})$
- efficiency:  $\widehat{B}_{OLS}$  satisfies that  $\sqrt{n} \operatorname{vec}(\widehat{B}_{OLS} B_{TRUE}) \rightarrow N(0, U_{OLS})$ , and  $U_{ENV} \leq U_{OLS}$



# Simulation

Т	rue signal	OLS	Envelope	OLS	Envelope	OLS	Envelope
20 40 60							•
	20 40 60	SNR = 0.01	SNR = 0.01	SNR = 0.1	SNR = 0.1	SNR = 1	SNR = 1
20 40 60	<b>•</b> 20 40 60	SNR = 0.01	● SNR = 0.01	SNR = 0.1	+ SNR = 0.1	<b>SNR</b> = 1	<b>+</b> SNR = 1
20 40 60	20 40 60	SNR = 0.01	<b>SNR</b> = 0.01	SNR = 0.1	<b>SNR</b> = 0.1	<b>SNR</b> = 1	• SNR = 1
20 40 60	20 40 60	SNR = 0.01	SNR = 0.01	SNR = 0.1	<b>L</b> SNR = 0.1	<b>L</b> SNR = 1	SNR = 1

#### **ADHD** analysis



Figure: The *p*-value map, thresholded at 0.05, using the OLS and envelope method with varying working dimensions. BIC selected (9, 10, 2).

findings: superior temporal gyrus, and pyramid and uvula in cereberter

# Sparsity and low-rankness



# Model

► model:

#### $oldsymbol{Y} = oldsymbol{B} imes_{(D+1)} oldsymbol{X} + arepsilon$

- Y ∈ ℝ<sup>r<sub>1</sub>×···×r<sub>D</sub></sup> = Dth-order array-valued response; can naturally handle both a general tensor and a symmetric tensor
- $\pmb{X} \in {\rm I\!R}^p = {
  m group}$  indicator, plus additional covariates like age, gender
- B ∈ ℝ<sup>r<sub>1</sub>×···×r<sub>D</sub>×p</sup> = (D + 1)th-order coefficient tensor that captures the interrelation between Y and X, and is our parameter of interest
- $\times_{(m+1)}$  is the (m+1)-mode product of the tensor **B** and vector **X**
- $\varepsilon \in \mathbb{R}^{r_1 \times \cdots r_D} = m$ th-order error tensor independent of X (no Kronecker product structure imposed)



Iow-rank structure:

$$\boldsymbol{B} = \sum_{k=1}^{K} w_k \boldsymbol{\beta}_{k,1} \circ \cdots \circ \boldsymbol{\beta}_{k,D} \circ \boldsymbol{\beta}_{k,D+1}$$

where  $w_k \in \mathbb{R}, \beta_{k,d} \in \mathbb{R}^d, \|\beta_{k,d}\|_2 = 1$ , and  $\beta_{k,D+1} \in \mathbb{R}^p$  encodes the predictor effect



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• for D = 2, K = 1,  $B = [[B_1, B_2]]$ ,  $B_1 = \beta_1$ ,  $B_2 = \beta_2$ ,  $B = w_1 \beta_1 \circ \beta_2$ • for D = 2, K = 2,  $B = [[B_1, B_2]]$ ,  $B_1 = [\beta_1^{(1)}, \beta_1^{(2)}]$ ,  $B_2 = [\beta_2^{(1)}, \beta_2^{(2)}]$ ,  $B = w_1 \beta_1^{(1)} \circ \beta_2^{(1)} + w_2 \beta_1^{(2)} \circ \beta_2^{(2)}$ 



Iow-rank structure:



- number of free parameters:
  - before:  $p \prod_{d=1}^{D} r_d$
  - after:  $K(p + \sum_{d=1}^{D} r_d)$
  - difference:  $p \prod_{d=1}^{D} r_d K(p + \sum_{d=1}^{D} r_d)$



Iow-rank structure:



▶ number of free parameters: — e.g.,  $r_1 = r_2 = r^3 = 64, K = 3, p = 3$ 

- before:  $p \prod_{d=1}^{D} r_d$  786, 432
- after:  $K(p + \sum_{d=1}^{D} r_d) 585$
- difference:  $p \prod_{d=1}^{D} r_d K(p + \sum_{d=1}^{D} r_d)$  save 785,847 parameters



Iow-rank structure:



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- difference:  $p \prod_{d=1}^{D} r_d K(p + \sum_{d=1}^{D} r_d)$  save 785,847 parameters
- entry-wise sparsity:

$$\|oldsymbol{eta}_{k,d}\|_0 \leq s_d, \quad 1 \leq d \leq D$$

- facilitate the interpretation
- ▶ no sparsity constraint on β<sub>k,D+1</sub>



#### Estimation

objective function:

$$\min_{\substack{w_k,\beta_{k,1},\dots,\beta_{k,D+1}}} \frac{1}{n} \sum_{i=1}^n \left\| \boldsymbol{Y}_i - \sum_{k=1}^K w_k (\boldsymbol{\beta}_{k,D+1}^{\mathsf{T}} \boldsymbol{X}_i) \boldsymbol{\beta}_{k,1} \circ \dots \circ \boldsymbol{\beta}_{k,D} \right\|_F^2,$$
subject to  $\|\boldsymbol{\beta}_{k,d}\|_2 = 1, \|\boldsymbol{\beta}_{k,d}\|_0 \leq s_d$ 

alternating updating algorithm: thanks to the bi-convexity

- ▶ update {w<sub>k</sub>, β<sub>k,1</sub>,..., β<sub>k,D</sub>}: solved by a hard-thresholding sparse tensor decomposition method
- update  $\beta_{k,D+1}$ : closed form solution
- ▶ symmetry can be obtained by setting  $\beta_{k,1} = \dots \beta_{k,D} = \beta_k$
- rank estimation: a variant of BIC



#### Theory

non-asymptotic error bound:



- for the actual minimizer obtained from our optimization algorithm, instead of a global minimizer that is not guaranteed to obtain
- interplay between the computational efficiency and the statistical rate of convergence, i.e., the computational error decays geometrically with the iteration number t, whereas the statistical error remains the same when t grows
- choose the maximal number of iterations T, such that the computational error is dominated by the statistical error
- the result holds for any distribution of the error tensor; further results when ε<sub>i</sub> is a Gaussian tensor, or a symmetric matrix



### Simulation





# Simulation





# **ASD** analysis



▶ findings: cerebellum, superior parietal lobule, precuneus



# **ASD** analysis



findings: left middle frontal gyrus, temporal lobe



# Thank You!

